Basic principles of MR imaging

Hoofdstuk 2: MR principe

Magnetische eigenschappen kern

Alle kernen met een ongelijke atomaire massa hebben een spin. Wanneer er een magnetisch veld aangezet wordt zullen deze spins ofwel parallel of antiparallel draaien. De spin vectoren draaien om een as met een specifiek frequentie => Larmor precessie. Er zullen net wat meer spins parallel aan het veld staan.

Larmor precessie

Door de spins aan te slaan met een RF puls van dezelfde frequentie als de spin. klapt de netto magnetisatie vector (M_s) om. Hierna draait de M_s met de Larmor frequentie in het magnetisch veld. Door het toevoegen van een ander magnetisch veld klapt de M_s om in de M_s, richting. Pliphoek = yB₁t. M_s is longitudinaal. M_s, is transversaal. Het maximale MR signaal ontstaat bij een 90° hoek. Een hogere veldsterkte leidt tot een hogere M_s en mogelijk een hoger signaal. M_s is statisch en geeft dus geen signaal.

Relaxatie

Na excitatie keren M, en M, terug naar de evenwichtstoestand waarbij elektromagnetische radiatie uitgezonden wordt. Beide relaxatie processen zijn onafhankelijk van elkaar, maar wel afhankelijk van moleculaire structuur, fysische staat en temperatuur.

- Longitudinale relaxatie: T₁ is een tijdconstante welke de tijd beschrijft die nodig is om terug te groeien tot 63% van de originele M, waarde. Grote en kleine moleculen hebben een relatief lange T₁ en medium moleculen een korte T₁. De T₁ van vloeistoffen is over het algemeen korten dan die van vaste stoffen. De T₁ is afhankelijk van hoe efficiënt energie uitwisseling plaats kan vinden. De T₁ gaat omlaag in de aanwezigheid van macromoleculen. 5x T₁ ~ 100% terug groei.
- Transversale relaxatie: T₂ is een tijdconstante voor spin-spin interacties om terug te vallen tot 37%. Door spin-spin interacties ontstaan er veld inhomogeniteiten, de spins defaseren en de M₂, neemt af. Vaste stoffen en grote moleculen hebben een korte T₂. Kleine moleculen hebben een korte T₂ en de aanwezigheid van macromoleculen verkort de T₃. De combinatie T₃ relaxatie en veld inhomogeniteiten wordt T₃* genoemd.

Free induction decay, signaal detectie en Fourier transformatie

Na de 90° puls wordt een signaal gemeten in een ontvangstspoel nadat de excitatie puls uit is gezet. Dit signaal wordt het 'free induction decay' signaal genoemd omdat het in de loop van de tijd vervalt. Het signaal oscilleert rond de Larmor frequentie, de amplitude daalt met T_2 * en door het uitvoeren van Fourier transformaties ontstaat het NMR spectrum. Amplitude $M_{\rm xy}$ is afhankelijk van proton dichtheid. Fourier transformeerd een functie in het tijddomein naar een functie in het frequentiedomein door integreren. Een rechthoek in de Fourier is een $\sin(\pi k)/\pi k = \sin(k)$.

Spin echo

De statische veld inhomogeniteiten kunnen teniet gedaan worden door de echo te meten i.p.v. het FID signaal. De 90° puls zorgt voor omklapping naar het XY-vlak. Door T₂ effecten treedt defasering op. Op TE/2 wordt een 180° puls gegeven waardoor de spins gespiegeld worden. De spins refaseren en vormen een echo. De spins zijn nu alleen nog van elkaar gescheiden door spin-spin interacties. Uiteindelijk wordt de echo hierdoor 0. De afname in amplitude is gelijk aan T₂. Scan duur = N₂ * TR. Vullen k-ruimte: G₂ en G₃ tegelijkertijd dus diagonaal _m 180° puls spiegeld in x=y _m G₄ individueel zorgt voor horizontale lijn.

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SB Merriam

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Basics of Magnetic Resonance Imaging William Oldendorf, William Oldendorf Jr., 1988-01-31 This book is not intended as a general text on MRI It is written as an intro duction to the field for nonexperts We present here a simple exposition of certain aspects of MRI that are important to understand to use this valuable diagnostic tool intelligently in a clinical setting The basic principles are presented nonmathematically using no equations and a minimum of symbols and abbreviations For those requiring a deeper understanding of MRI this book will help facilitate the transition to standard texts Chapters 1 through 4 provide a general introduction to the phenomenon of nuclear magnetic resonance and how it is used in imaging Chapter 1 discus ses magnetic resonance using a compass needle as an example In Chapter 2 the transition to the magnetic resonance of the atomic nucleus is made Chapter 3 describes the principles of imaging In Chapter 4 the terms T 1 and T 2 are described and their relationship to tissue characterization the fun damental role of thermal magnetic noise in T 1 and T 2 Introduction to Functional Magnetic Resonance Imaging Richard B. Buxton, 2002-01-07 Functional Magnetic is discussed Resonance Imaging fMRI is now a standard tool for mapping activation patterns in the human brain This highly interdisciplinary field involves neuroscientists and physicists as well as clinicians who need to understand the rapidly increasing range flexibility and sophistication of the techniques In this book Richard Buxton a leading authority on fMRI provides an invaluable introduction for this readership to how fMRI works from basic principles and the underlying physics and physiology to newer techniques such as arterial spin labeling and diffusion tensor imaging **Magnetic Resonance Imaging** Stewart C. Bushong, 2003 Magnetic Resonance Imaging presents the fundamentals and principles of MRI its capabilities and various applications MRI can be a difficult subject because the physical principles underlying MRI are different from those of x ray imaging This text provides a clear and comprehensive explanation of the basic principles of conventional MRI and of the fast imaging techniques currently available Over 450 images photos and line drawings accompany each discussion clarifying difficult material Easy to read comprehensive material addresses six important content areas in an engaging style that does not require an extensive background in math or physics but still goes beyond superficial coverage Appendices provide more complex mathematical content in The Bloch Equations as well as a list of web addresses for professional organizations scientific associations and other sources of information relevant to the topics in the book New chapters on Chemical Shift and Magnetization Transfer chapter 19 Perfusion Imaging chapter 24 Diffusion Imaging chapter

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